

Multifunctional Magnetic Mesoporous Silica Nanoagents for *in vivo* Enzyme-Responsive Drug Delivery and MR Imaging

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Abstract

In this study, we report novel multifunctional nanoagents for *in vivo* enzyme-responsive anticancer drug delivery and magnetic resonance imaging (MRI), based on mesoporous silica coated iron oxide nanoparticles ($\text{Fe}_3\text{O}_4@\text{MSNs}$). The anticancer drug, DOX, was encapsulated in the porous cavities with a MMP-2 enzyme responsive peptide being covalently linked to the nanoparticles surface. The *in vitro* experiment results indicated that the enzyme responsive nanoagents own high specificity for controlled drug release in the cell line with high MMP-2 expression. Furthermore, the targeted delivery of the nanoagents to the tumor site purpose has been successfully achieved through magnet-guided nanocarrier accumulation by utilizing the magnetic properties of the Fe_3O_4 nanocores, which resulted in efficient inhibition of the tumor growth. Additionally, these novel nanoagents can also be used as MRI agent for the real-time diagnosis the tumor treatment process of living animals. Taking the advantages of high specificity, controllable drug release and real-time MRI imaging, we believe these multifunctional nanoagents could also be used as a general platform for the design of stimulus-responsive multifunctional nanomaterials for the aim of accurate diagnosis and efficient treatment of other diseases.

Key words: iron oxide, enzyme-responsive drug delivery, tumor inhibition

Introduction

Cancer keeps being one of the extremely complex diseases that challenge the lives of human beings in all age groups [1]. So far, several standard approaches have been well developed for cancer therapy, such as chemotherapies and surgery [2]. Although traditional chemotherapy has been proved to be effective, it faces the primary concerns of systematic toxicity of drug molecules and poor tumor selectivity, which cause damage to healthy tissues [3].

Accounting targeted chemotherapy, the major issue is its incapability to specially deliver the sufficient amount of therapeutic reagents to the disease area [4]. Although surgery is the preferred treatment method for many cancers, it is difficult to unambiguously distinguish between normal and cancer tissues during treatment. It remains to be a big challenge to achieve complete removal of cancer tissues and minimize recurrences. Thus, the rational design that can

effectively deliver sufficient drug molecules to the disease site has always attracted enormous research interest.

To date, various strategies have been developed for targeted drug delivery through controlling the drug release to the tumor [5-7]. Taking the advantages of nanotechnology, many different kinds of bio-inspired and stimuli-responsive (such as pH, ionic strength, light, enzyme, etc) systems have been exploited for therapeutic agent delivery [8-11]. As well known, enzymes play critical roles in activating almost all biological processes, thus the dysregulation of enzyme expression and activity underpins the pathology of many diseases, which could be employed for the design of enzyme-responsive drug delivery system [12-14]. The integration of nanomaterials with responsive enzymatic system can endow the formulations of bio-specificity and selectivity, constituting new possibilities for promising applications in targeted drug delivery [15]. Especially for tumor treatment, those enzymes that intimately associated with tumor invasiveness and metastasis (such as protease and phospholipases) are important candidates to be utilized for the design of tumor-targeted drug delivery systems [16-20].

Matrix metalloproteinases (MMPs), as one of the important internal physiological changes of the tumor microenvironment, is such an indicator protein that is overexpressed in almost all tumors [21]. It has been demonstrated that MMP-2 triggered nanocarriers can be used for cancer imaging and therapy with high specificity and sensitivity [22, 23]. For instance, Peng et al. designed a N-(2-hydroxypropyl)-methacrylamide (HPMA) copolymer system with MMP-2 cleavable spacer for targeted drug delivery of prostate cancer therapy [24]. Zou and co-workers demonstrated a MMP-2 responsive system for tumor drug release by using gelatin layer blocked nanocarrier [25]. However, the drug delivery platforms employed in these designs typically require complicated synthetic processes which become the

main obstacle for their practical applications. Accounting these, the rational design of a simple and effective strategy that enables tumor-targeted therapy is highly expected.

So far, the mesoporous silica-related nanostructures have attracted great research interest in therapeutic applications because of their active surface for drug loading, good biocompatibility and convenient surface modification [26-28]. Accordingly, enormous research efforts have been devoted to the advancement of multifunctional mesoporous silica-based nanoplatfoms (MSNs) for therapeutic applications. For instance, using β -CD capped MSNs, Hu et al. proposed a ROS-triggered drug release system for enhanced chemotherapy [29]. Zhao et al. have demonstrated that the mitochondria targeted MSNs can effectively deliver the anticancer agent, α -tocopheryl succinate, with enhanced efficiency.[30] Zhao's group has also demonstrated that the dyes loaded inside MSNs can be effectively protected from nucleophilic attack, thus the hybrid presents significant potential for fluorescence imaging *in vitro* [30, 31].

Taking the aforementioned advantages of MSNs, in this study, we propose a new strategy for targeted drug delivery based on the multifunctional mesoporous silica coated iron oxide nanoagents (Fe_3O_4 @MSNs, Figure 1). The surface of Fe_3O_4 @MSNs was further modified by the MMP-2 responded peptide substrate (PLGVR). We demonstrate that this peptide- Fe_3O_4 @MSNs drug delivery system enables the real-time monitoring of the cellular drug release in living conditions as well as for fluorescence imaging and magnetic resonance imaging (MRI). *In vivo* animal tests on tumor-bearing mouse model further reveal the efficient and targeted drug release at the tumor site. Compare with previously published drug delivery carriers that used for MRI, fluorescence imaging and drug delivery [32-34], Fe_3O_4 @MSNs provide magnetic targeting as a complementary mean nanoparticles' enrichment in the tumor area, whereas

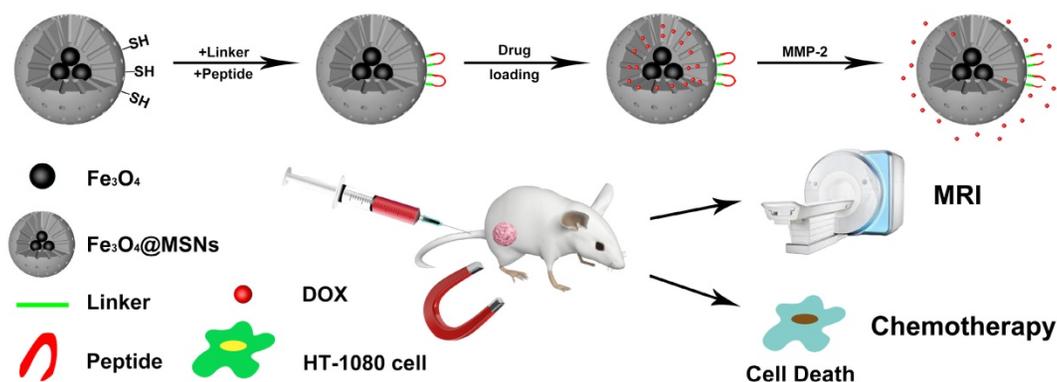


Figure 1. Schematic illustration of peptide- Fe_3O_4 @MSNs for enzyme-responsive drug delivery and MRI

effective enrichment is of great importance to drug carriers. In addition, these multifunctional nanoagents could also be used as a general platform for the design and fabrication of enzyme responsive functional nanomaterials that offer new possibilities to diagnose and combat with cancer.

Materials and Methods

Materials

Sodium oleate (>95%), iron chloride (>99%), oleic acid (>99%), ethyl acetate (>99%), N, N-Dimethylformamide (DMF) (>99%) and dimethyl sulfoxide (DMSO) (>99%) were purchased from Sinopharm group CO. Ltd. Cetyltrimethylammonium bromide (CTAB) was purchased from Sigma-Aldrich. Tetraethyl orthosilicate (TEOS) (>99%), (3-mercaptopropyl)-methyl dimethoxysilane (>99%), 1-octadecene (ODE) (90%), 3-(Maleimido) propionic acid N-hydroxysuccinimide ester (NHS-linker) (99%) and doxorubicin (DOX) (>98%) were purchased from Aladdin. MMP-2 peptide (Gly-Gly-Pro-Leu-Gly-Val-Arg-Gly-Lys) (96.17%) was provided by China Peptides Co., Ltd.

Synthesis of Fe₃O₄@MSNs

Oleic acid coated Fe₃O₄ nanoparticles were prepared following the method [35]. In typical experiments, iron oleate (1.0 g) and oleic acid (177.3 μL) were added into ODE (7.1 mL). The mixture was stirred at 120 °C for 1 h and then heated to 312 °C under N₂ atmosphere followed by maintained for another 1 h. After cooling down to room temperature and precipitation through adding extra ethanol, the Fe₃O₄ nanoparticles were collected by centrifugation. The products were then washed with hexane and ethanol and stored for the further use.

To transfer Fe₃O₄ nanoparticles into aqueous phase, dispersion of nanoparticles (1.0 mL in chloroform) was mixed with the CTAB solution (0.4 g in 20 mL DI water) and then stirred at 60 °C for 3 h. After that, the mixture was filtered through 0.44 μm syringe filter to remove large aggregates. The filtered solution (2.5 mL) and NaOH (2 M, 175 μL) solution were diluted with deionized water (21.5 mL), followed by heating to 70 °C. After stirring for 10 min at 70 °C, TEOS (150 μL) and ethyl acetate (1.5 mL) were added into the mixture. After stirring for another 5 min, (3-mercaptopropyl)-methyl dimethoxysilane (12.5 μL) was added to the mixture. The Fe₃O₄@MSNs were collected after 3 h washed by ethanol for three times. Then precipitation was re-dispersed in ethanol and mixed with NH₄NO₃ (80 mg) at 60 °C and stirred for 2 h to remove the excess CTAB. The morphology and size distribution of those particles were examined using a transmission electron

microscope (Tecnai G220, FEL, USA) at an acceleration voltage of 200 kV. MR relaxometry of the magnetic Fe₃O₄@MSNs particles was performed using a 3.0 T MRI equipment (GE 3.0 T Signa) and T₂ relaxivity was deduced from inverse T₂ as a function of iron concentrations.

Synthesis of peptide-Fe₃O₄@MSNs

Fe₃O₄@MSNs (17.0 mg) and NHS-linker (23.5 mg) were mixed with DMF (360 μL) and followed by adding DIPEA (15 μL). The reaction was left to stir for 12 h at room temperature. The product was collected through centrifugation and washed with ethanol for three times. After being re-dispersed in DMF (360 μL), the peptide (15.0 mg) and DIPEA (10 μL) was added and stirred for another 12 h. After that, the reaction solution was centrifuged to remove unreacted reactant and then washed with ethanol/water (1:1) for three times. The final product was suspended in dried dimethyl sulfoxide (DMSO) for further use.

Drug loading on peptide-Fe₃O₄@MSNs nanocarriers

200 μL DOX in DMSO (10 mg/mL) was mixed with 3.7 mg peptide-Fe₃O₄@MSNs. The mixture was stirred for 24 h in the dark environment. The nanoparticles were collected by centrifugation and the precipitation was washed with PBS buffer for three times to remove the excess DOX. All the supernatant was collected for measuring the UV absorbance of DOX, which was used to evaluate the loading efficiency of DOX by peptide-Fe₃O₄@MSNs. The final product was abbreviated as peptide-Fe₃O₄@MSNs/DOX.

Drug release from peptide-Fe₃O₄@MSNs/DOX

2 μL of MMP-2 enzyme stock solution (200 ng/mL) was added to each vial containing peptide-Fe₃O₄@MSNs/DOX solution of Tris buffer (10 μM, 20 μL) and incubated for a series of times (20 min, 40 min, 60 min, 80 min, 100 min, 120 min, 140 min, 160 min) at 37 °C. After centrifugation, the supernatant was collected and then diluted with PBS buffer (80 μL). Fluorescence spectroscopic studies were performed at an excitation wavelength of 480 nm. Additionally, nanocarriers without peptide capping or the nanocarriers with additional inhibitor, were also explored as control experiments.

MTT assay

HT-1080 and NIH/3T3 cells were cultured in a 96-well culture plate at a density of 1×10⁴ cells per well under 5% CO₂ atmosphere condition at 37 °C for 24 h. Then, the cells were washed with PBS and incubated with Fe₃O₄@MSNs, peptide-Fe₃O₄@MSNs/

DOX, and free DOX (DOX concentration: 5 μ M), respectively. After incubation for 2 h, 4 h, 8 h, 12 h and 24 h, the original medium was replaced by 100 μ L medium containing 10 μ L MTT solution (5 mg/mL) and incubated for another 4 h. Then the medium was removed and followed by adding 100 μ L DMSO into each well to dissolve the precipitate. The absorption of each solution was measured at 490 nm on a microplate reader (Synergy NEO).

Laser scanning confocal microscopy

HT-1080 and NIH/3T3 cells were seeded to confocal dishes with a density of 1.5×10^5 per dish, respectively. 1 mL medium containing peptide- Fe_3O_4 @MSNs/DOX or free DOX (DOX concentration: 5 μ M) was added to each dish. After incubation for 4 h, 8 h and 12 h, the culture medium was replaced with PBS buffer. Then the Hoechst 33342 (10 μ g/mL) was added to stain the nuclei of cells. The confocal images were obtained using a laser scanning confocal microscope (OLYMPUS FV120).

Tumor-bearing mice model

Animal experiments were conducted strictly following the guidelines of the Institutional Animal Care and Use Ethical Committee of Soochow University. Female nude mice of 5 weeks old were purchased from Shanghai SLAC Laboratory Animal Co. Ltd (Shanghai, China). The tumor model was established by subcutaneously injecting 100 μ L PBS containing 3×10^6 HT-1080 cells into the back of each mouse. After around 2 weeks, the mice bearing 100 mm^3 tumors were selected for following experiments.

Biodistribution analysis

Tumor-bearing mice were randomly divided into two groups, which were intravenously injected with (1) peptide- Fe_3O_4 @MSNs/DOX (2 mg/mL, 200 μ L; 1.6 mg/kg), and (2) peptide- Fe_3O_4 @MSNs/DOX (2 mg/mL, 200 μ L, 1.6 mg/kg) with magnet treatment, respectively. For the bio-distribution assay: the mice were humanely sacrificed after 8 h. After that, the main organs, tissues and tumors were collected, wet-weighed, and dissolved in the digesting solution (HNO_3 : H_2O_2 of 2:1 by volume). The content of iron ions in each tissue was determined by ICP-OES.

In vivo MR imaging

Tumor-bearing mice were injected with peptide- Fe_3O_4 @MSNs/DOX (2 mg/mL, 200 μ L; 1.6 mg/kg equiv DOX) via tail vein. In addition, magnetic targeting was applied to half of these mice. The MR images were captured by a T_2 -weighted spin-echo sequence (TR/TE =4000/108 ms; slice thickness, 2 mm; slice spacing, 1 mm; matrix, 256 \times

256; FOV, 8 cm \times 8 cm). Signal variation was observed after the injection of nanocarriers for 0.5 h, 1 h, 2 h, and 3 h.

In vivo chemotherapy

The tumor-bearing mice were randomly divided into 3 groups (each group has 5 mice): (1) control group (treated with PBS), (2) peptide- Fe_3O_4 @MSNs/DOX group, and (3) peptide- Fe_3O_4 @MSNs/DOX & magnet group. Mice in experimental groups were injected with nanocarriers (2 mg/mL, 200 μ L, 1.6 mg/kg equiv DOX, freshly prepared) through the tail vein every two days. For peptide- Fe_3O_4 @MSNs/DOX & magnet group, magnetic treatment at the tumor site was conducted for 8 h after each injection. The body weight and tumor size of each mouse were measured every two days. The tumor volumetric size was calculated according to the formula: $V=LW^2/2$ (V : the volume of tumor, L : the maximum length of the tumor, W : the minimum width of the tumor). After 3 weeks of treatment, all mice were sacrificed and main organs were collected for histological analysis.

Histological analysis

For the hematoxylin and eosin (H&E) staining experiment, the major organs (heart, liver, spleen, lung, and kidney) that were collected from previous step were harvested, dipped in 10% formalin and processed routinely into paraffin. Then the 5 μ M thick slices were prepared and stained with H&E for histological analysis.

Results and Discussion

The core-shell Fe_3O_4 @MSNs was synthesized via the sol-gel reaction method [36, 37]. The hydrophobic spherical Fe_3O_4 nanoparticles were prepared following the method [35]. To enhance the biocompatibility and the subsequent drug loading efficiency, the Fe_3O_4 nanoparticles obtained were coated with thiol-modified mesoporous silica shell. TEM was used to characterize the morphologies of Fe_3O_4 and Fe_3O_4 @MSNs nanoparticles. As shown in Figure 2a and 2b, Fe_3O_4 and Fe_3O_4 @MSNs had a spherical shape and uniform size. Average sizes of Fe_3O_4 and Fe_3O_4 @MSNs were determined by counting more than 200 nanocrystals per sample, which were 14 nm and 114 nm, respectively (Figure S1a and 1b). The dynamic light scattering (DLS) measurements, shown in Figure S1c, revealed that the hydrodynamic size of Fe_3O_4 @MSNs dispersed in PBS was around 600 nm. More importantly, after three rounds of testing, the location of peaks varied slightly, meaning that Fe_3O_4 @MSNs had excellent colloidal stability, which was very important for their biomedical applications. It is clear that the silica coating layer is around 50 nm

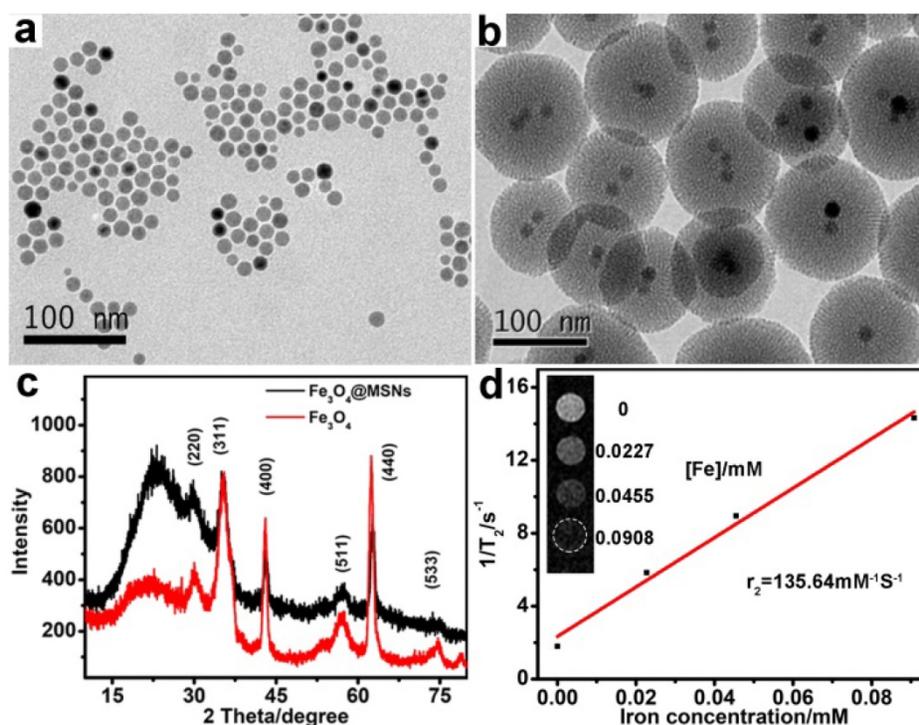


Figure 2. TEM images of (a) Fe₃O₄ and (b) Fe₃O₄@MSNs. (c) XRD pattern of Fe₃O₄ and Fe₃O₄@MSNs. (d) T₂-weight MR images of Fe₃O₄@MSNs at different iron concentration and plot of T₂⁻¹ versus iron concentration. Transverse (r₂) relaxivity was derived from linear fitting of the data.

thick, which provides an attractive cavity for drug loading. The phase purity of the as-synthesized Fe₃O₄ and Fe₃O₄@MSNs were further characterized through XRD (Figure 2c), which indicated that pure Fe₃O₄ was obtained (PDF# 19-0629) [38] and the successful coating of Fe₃O₄ by amorphous silica. The contrast effect of the Fe₃O₄@MSNs was verified by measuring transverse (T₂) relaxation times of dispersed nanostructures on the 3.0 T MRI equipment (TR 4240 ms; TE 108 ms; slice thickness, 1 mm; slice spacing, 1 mm; matrix, 256 × 256; FOV, 8 cm × 8 cm). The T₂-weight MR signals were significantly enhanced with the rise of concentration of nanomaterials. The specific relaxivity value (r₂) was calculated to be 135.6 mM⁻¹ s⁻¹ (Figure 2d), indicating that the Fe₃O₄@MSNs can serve as sensitive contrast agent for MRI [39].

For the purpose of efficient drug encapsulation and enhanced tumor targeting of the nanocarriers, the surface of the silica shell was further covalently capped with the MMP-2 substrate peptide (GGPLGVRGK). The drug loading capability of this peptide-Fe₃O₄@MSNs platform was evaluated with the commercial anticancer drug, DOX. Typically, the peptide-Fe₃O₄@MSNs was soaked in a DOX/DMSO mixed solution for 24 h, then the nanocarriers were centrifuged to remove the unbound DOX and the precipitate was further washed by PBS (10 mM, pH=7.2). The loading efficiency was determined by the difference in the UV-Vis absorbance of DOX at 480 nm, which was calculated to be 12.2% (w/w). This value was comparable with the results reported

previously [33, 40]. Generally, DOX exhibited a red fluorescence emission under excitation at 480 nm, while peptide-Fe₃O₄@MSNs/DOX showed almost undetectable fluorescence (Figure 3a). Similarly, after centrifugation, the tube containing peptide-Fe₃O₄@MSNs/DOX showed significantly weaker fluorescent signal compared with the tube with free DOX (Figure 3a, insert graph). This is because the fluorescence is quenched when the DOX molecules were encapsulated into mesoporous silica shell, because of self-quenching [10, 41].

To verify the efficiency of this enzyme-responsive drug delivery system, the drug release test was experimentally carried out under physiological condition (Tris buffer, 37 °C). The following samples were prepared as control: (1) Fe₃O₄@MSNs/DOX sample without peptide capsulation; (2) peptide-Fe₃O₄@MSNs/DOX without enzyme and (3) the peptide-Fe₃O₄@MSNs/DOX with enzyme and inhibitor (prinomastat hydrochloride). As shown in Figure 3b, in the first 20 min, the release rate of DOX from Fe₃O₄@MSNs/DOX increased dramatically which was much higher than other samples, because the porous surface was not blocked by anything. When it came to peptide-Fe₃O₄@MSNs/DOX with enzyme, the release rate was pretty low in the first 20 min. However, from 20 min to 80 min, the profile underwent a quick increase and nearly 70% (comparable to that of Fe₃O₄@MSNs/DOX) of DOX escaped from peptide-Fe₃O₄@MSNs/DOX. This is attributed to the MMP-2 enzyme which

cleaved the blocked peptide. In contrast, for the peptide-Fe₃O₄@MSNs/DOX sample in the presence of MMP-2 and inhibitor, only about 17% DOX was released even after 160 min. This value is very close to the release ratio of peptide-Fe₃O₄@MSNs/DOX only (about 15.7%). In addition, the fluorescent images of peptide-Fe₃O₄@MSNs/DOX solution incubated with MMP-2 enzyme or MMP-2 and enzyme inhibitor at different time were also exhibited in the insert of Figure 3b. It is clear that, for samples treated with MMP-2 only, the strength of fluorescence signal gradually increased with respect to incubation time. In contrast, very weak signal intensity change was detected for samples treated with MMP-2 and inhibitor together. These results solidly support the high performance of this peptide-Fe₃O₄@MSNs/DOX nanocarrier system for enzyme-responsive drug release, both in release efficiency and enzyme sensitivity.

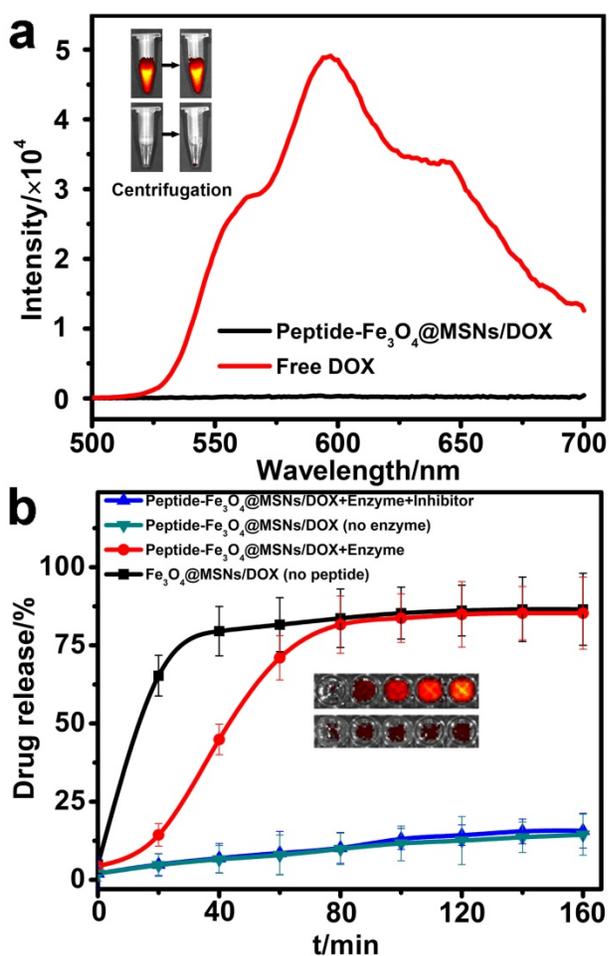


Figure 3. (a) Fluorescence spectrum of free DOX and peptide-Fe₃O₄@MSNs/DOX. Inset: corresponding fluorescence images of free DOX (upper) and peptide-Fe₃O₄@MSNs/DOX (nether) before (left) and after (right) centrifugation. (b) Enzyme-responsive release profiles of DOX from Fe₃O₄@MSNs/DOX, peptide-Fe₃O₄@MSNs/DOX (with and without MMP-2), peptide-Fe₃O₄@MSNs/DOX with MMP-2 and MMP-2 inhibitor. Inset: fluorescence images of peptide-Fe₃O₄@MSNs & MMP-2 (upper) and peptide-Fe₃O₄@MSNs & MMP-2 & inhibitor (nether) after different time (20 min, 40 min, 80 min, 120 min, 160 min, from left to right).

To assess the biocompatibility and the anticancer effect of the peptide-Fe₃O₄@MSNs/DOX system, two kinds of cells, HT-1080 (representing tumor cells) and NIH/3T3 (representing normal cells) were employed for cellular cytotoxicity test. The methylthiazolotetrazolium assay (MTT) was adopted to evaluate the anticancer effect. Typically, the HT-1080 cells and NIH/3T3 cells were incubated with Fe₃O₄@MSNs, peptide-Fe₃O₄@MSNs/DOX and free DOX for 2 h, 4 h, 8 h, 12 h and 24 h, respectively. The doses of DOX were kept being same between the peptide-Fe₃O₄@MSNs/DOX and free DOX. HT-1080 and NIH/3T3 cells without any treatment were selected as controls in this study. From Figure 4a and 4b, as high as 93.9% (HT-1080) and 92.9% (NIH/3T3) of cell viability were detected when they were cultured with Fe₃O₄@MSNs even after 24 h, indicating the considerably good biocompatibility of Fe₃O₄@MSNs. When NIH/3T3 cells were cultured with peptide-Fe₃O₄@MSNs/DOX, the cell viability still reached 80% after 24 h, which was higher than that treated with free DOX (46.4%, Figure 4a). While for HT-1080 cells treated with both peptide-Fe₃O₄@MSNs/DOX and free DOX, the cell viabilities were comparable, about 50% and 46% respectively (Figure 4b), which indicated the nanocarriers got a favourable selectivity between normal cells and cancer cells.

Utilizing the fluorescence property of DOX molecules, the nanocarrier distribution and drug release process in living cells were monitored by confocal fluorescence imaging. HT-1080 cells were used as representatives which were incubated with free DOX, peptide-Fe₃O₄@MSNs/DOX and peptide-Fe₃O₄@MSNs/DOX + inhibitor. The intracellular distribution of DOX and morphology change of cells nuclei were monitored with respect to incubation time. After incubation with free DOX for 4 h (Figure. 4c), clear deformation was detected for the morphology of cells and their nuclei. When the incubation time was prolonged to 8 h and 12 h respectively, a sharp decrease of the cell density happened, indicating clear cell death caused by free DOX. Meanwhile, for those cells treated with peptide-Fe₃O₄@MSNs/DOX (Figure 4d), DOX was mainly distributed in cytoplasm at 4 h. After incubation for another 4 h, significant deformation of cells was observed and the red fluorescence from DOX in the nucleus was detected. After 12 h incubation, the fluorescence signal of DOX was concentrated in the nucleus and the signal of cytoplasm was almost invisible. Simultaneously, the cell density was also decreased considerably. On the contrary, the HT-1080 cells cultured with peptide-Fe₃O₄@MSNs/DOX + inhibitor exhibited

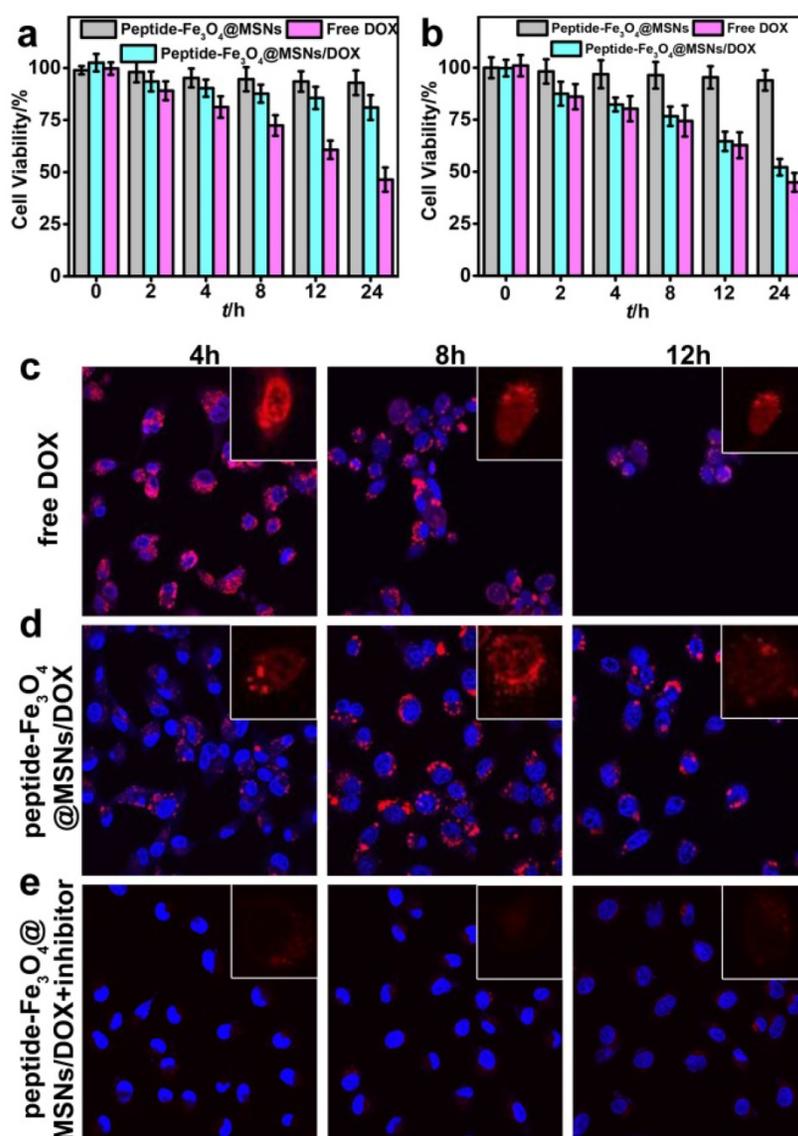


Figure 4. MTT assay of (a) NIH/3T3 cells and (b) HT-1080 cells with peptide-Fe₃O₄@MSNs, peptide-Fe₃O₄@MSNs/DOX and free DOX. Confocal images of HT-1080 cells incubated with free DOX (c), peptide-Fe₃O₄@MSNs/DOX (d) and peptide-Fe₃O₄@MSNs/DOX + inhibitor (e) for different time (4 h, 8 h, 12 h). (Inset: confocal images of single cells, only DOX fluorescence signal)

very weak red fluorescence in the cytoplasm even after 12 h incubation time and the cell density almost did not change (Figure 4e). On the other hand, NIH/3T3 cells treated with peptide-Fe₃O₄@MSNs/DOX did not show the red fluorescence in the first 4 h incubation and emitted very weak fluorescence signal after 12 h, which was attributed to the low expression of MMP-2 enzyme (Figure S2). These results showed that peptide-Fe₃O₄@MSNs/DOX nano-platform had high specificity to cancer cells with MMP-2 expression and limited toxicity to normal cells.

Before *in vivo* chemotherapy experiments, the biodistribution of peptide-Fe₃O₄@MSNs/DOX was tested to evaluate the targeting capability based on the dual roles of magnetic targeting and enhanced permeabilization and retention (EPR) effect. Tumor-bearing mice were randomly divided into two

groups (3 mice in each group) and both groups were intravenously injected with peptide-Fe₃O₄@MSNs. After 8 h, both groups were humanely sacrificed to collect the organs and tumor tissues to check the distribution of iron ion in each part through ICP-OES. These results are summarized in Figure S3. Firstly, it is found that the nanocarriers accumulated in the reticuloendothelial organs like liver and spleen which was a common feature for nanomaterials in previous studies [42]. Secondly, tumor uptake of peptide-Fe₃O₄@MSNs through passive targeting was much lower than that treated with magnet. This phenomenon indicates that magnetic-guided delivery can effectively promote the enrichment of nanocarriers in tumor site and could be used to improve the treatment efficiency.

Confocal images were used to evaluate the *in vivo* efficiency of enzyme-responsive release of peptide-Fe₃O₄@MSNs/DOX. In control experiment of mouse injected with free DOX (Figure S4), there was always a strong fluorescence signal no matter at 0.5 h or 2 h. In contrast, for mouse injected with peptide-Fe₃O₄@MSNs/DOX, a very weak signal was detected at 0.5 h. The signal kept increasing and was considerably strong at 2 h after injection, reflecting that the DOX was successfully and sufficiently released *in vivo*. However, if mouse was pre-treated with inhibitor, almost no fluorescence could be observed even after 2 h treatment. The *in vivo* results are well consistent with the findings of the confocal imaging and biodistribution analyses, which indicated the high efficiency of peptide-Fe₃O₄@MSNs/DOX for magnetic-guided targeted delivery.

MRI is one important non-invasive imaging technique for tumor diagnosis. Herein, taking the magnetic property of Fe₃O₄ core, the peptide-Fe₃O₄@MSNs/DOX system could serve as an efficient contrast agent for T₂-weight MRI. The results are summarized in Figure 5a and 5b. It was found that for

tumor site without magnet treatment (Figure 5a), only a faint darkening was detected at tumor area after injection for 3 h. Simultaneously, for mice treated with additional magnet for 3 h (Figure 5b), a clear darkening was found, indicating that magnetic guiding could effectively induce the accumulation of drug nanocarriers to the tumor site.

To access the efficiency of *in vivo* chemotherapy, firstly we summarized the photos of mice after 21 days treatment of three parallel treatments in Figure 5c which revealed quite different phenomenon. For mice injected with PBS only (the control), the tumor became significantly larger because of its continuous growing. Meanwhile, the tumor had smaller size for mice treated with peptide-Fe₃O₄@MSNs/DOX. Amongst three tests, the peptide-Fe₃O₄@MSNs/DOX & magnet group had the smallest tumor size, indicating the successful suppression of tumor growth. The time evolutions of body weight and tumor size were quantitatively evaluated and summarized in Figure 5d and Figure 5e. During the treatment, the body weights almost kept being constants, except that slight decrease were observed

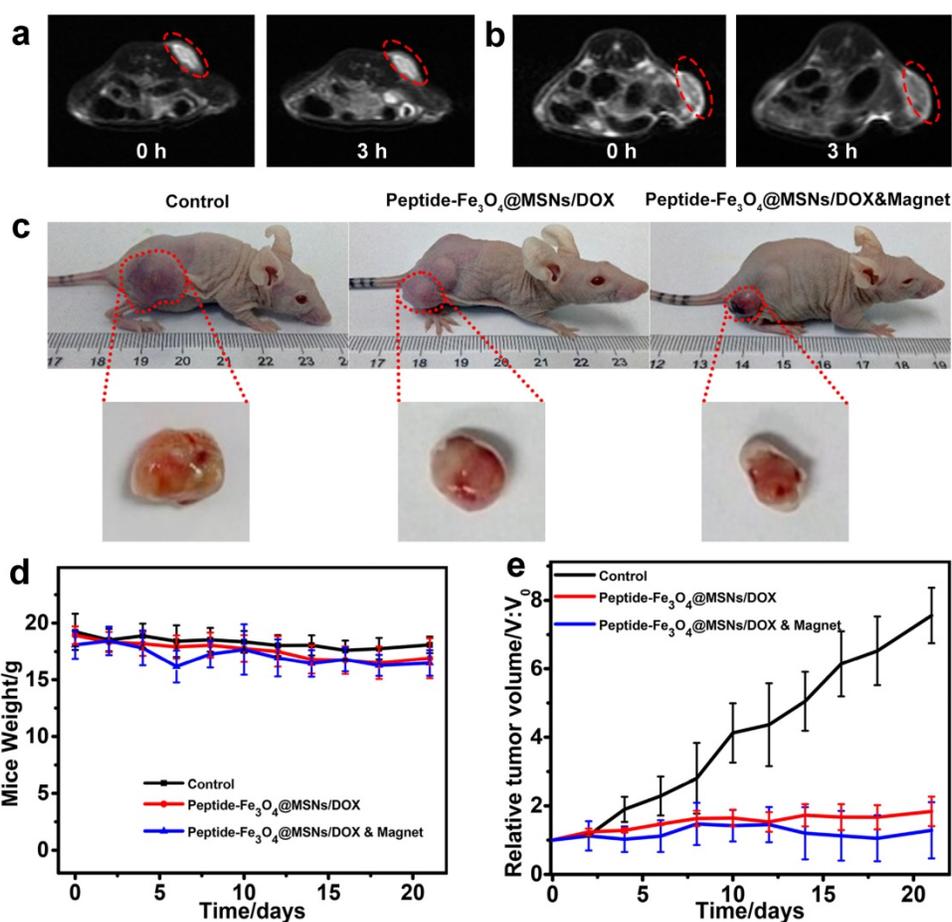


Figure 5. *In vivo* MRI (T₂-weight) images of tumor (a) treated with peptide-Fe₃O₄@MSNs/DOX (images were taken 0 h and 3 h after injection), (b) treated with peptide-Fe₃O₄@MSNs/DOX & magnet (images were taken 0 h after injection and 3 h magnet treatment at the tumor site). (c) Photographs of mice without treatment (left), with Peptide-Fe₃O₄@MSNs/DOX (middle) and Peptide-Fe₃O₄@MSNs/DOX & Magnet (right) treatment for 21 days. The collected tumor tissues are depicted at the bottom of each figure. (d) Body weight curves of different groups for 21 days. (e) Tumor volume curves of different group for 21 days.

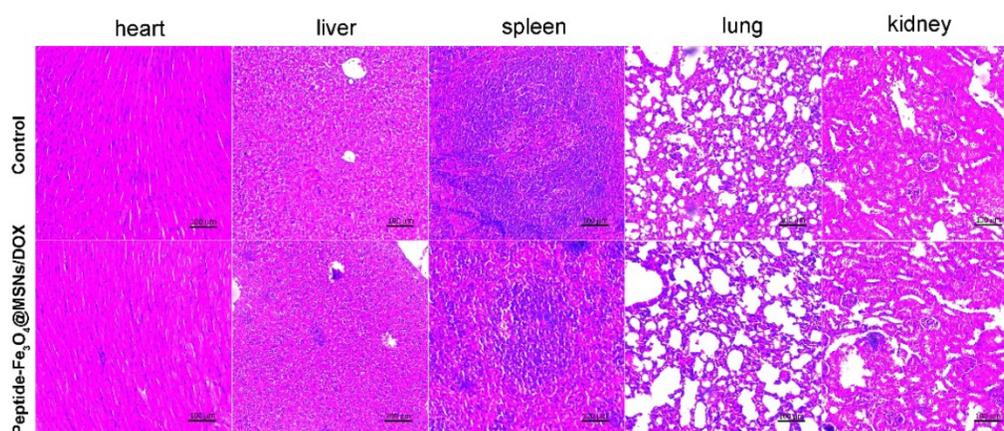


Figure 6. H&E stained images of major organs harvested from control mice and mice treated with peptide-Fe₃O₄@MSNs/DOX, samples were collected three weeks after treatment.

for the two groups with the treatment of nanocarriers. This was mainly attributed to the side effect of chemotherapy. The tumor volumetric size of the control group increased dramatically to be more than 7 times of the primary size. On the contrary, the tumor only increased to be around 1.7 times for that treated with peptide-Fe₃O₄@MSNs/DOX. With additional magnet treatment, the tumor size was almost unchanged which was in line with the findings in Figure 5c, meaning that peptide-Fe₃O₄@MSNs/DOX system could effectively inhibit tumor growth.

The main organs were then collected for pathological analysis to evaluate the *in vivo* toxicity of the nanocarrier system. As shown in Figure 6, only a slight edema was found in liver of mice treated with nanocarriers, indicating favourable biosafety in living system. This is benefitted to the silica coatings which are principally accepted to be safe. These results also confirmed the effectiveness of magnetic guided nanocarrier accumulation used as a supplementary approach for tumor treatment by magnetic nanoparticles.

Conclusions

In summary, an enzyme-responsive drug delivery nanosystem based on mesoporous silica coated magnetic iron oxide nanoparticles (Fe₃O₄@MSNs) has been constructed for MRI-guided cancer chemotherapy. By capping the mesoporous silica shell with MMP-2 substrate peptide, the functionalized peptide-Fe₃O₄@MSNs can effectively encapsulate with anticancer drug. We demonstrated that, by adding the MMP-2 enzyme, the peptide on the nanoparticle surface could be efficiently cleaved to induce the drug molecules release both *in vitro* and *in vivo*. Moreover, the *in vitro* results indicated that the peptide-Fe₃O₄@MSNs/DOX own good biocompatibility and high specificity towards the cancerous cells with high MMP-2 enzyme expression. The *in vivo*

experiments demonstrated that this magnetic nanoagent could efficiently accumulate at the tumor site through the treatment of an external magnetic field. MRI-guided chemotherapy experiments further revealed the successful inhibition of tumor growth. In addition to the cancer chemotherapy, this nanoagents could also be used as a general platform for the design of stimulus-responsive functional nanomaterials that find fruitful applications in biomedical related areas.

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Supplementary Material

Supplementary figures.

<http://www.ntno.org/v02p0233s1.pdf>

Competing Interests

The authors have declared that no competing interest exists.

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